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(54) Title: A NEW SYSTEM FOR ADMINISTRATION OF LIPOSOMES TO MAMMALS		
(57) Abstract <p>A new system to administer liposomal formulations to mammals, including man, comprising a dry lipid-based solid material, which in an aqueous milieu spontaneously form or reconstitute liposomes, and a device for aerosolizing a selected quantity of the lipid-based solid material in a suitable form. The invention is particularly suitable for applications where the lipid-based solid composition is inhaled as a finely-divided powder in aerosol form and hydrated in the respiratory tract.</p>		

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A new system for administration of liposomes to mammals

DESCRIPTION

Field of invention

5 The present invention provides a new system to administer liposomal formulations to mammals, including man, comprising a dry lipid-based solid material, which in an aqueous milieu spontaneously form or reconstitute liposomes, and a device for aerosolizing a selected quantity of the dry lipid-based solid material in a suitable form. The invention is particularly concerned with breath-actuated powder-inhalators and self-propelling powder-dispensing compositions capable of dispensing in aerosol form a powder of said dry lipid-based solid materials.

15 Until now liposomal formulations have been administered to mammals as aqueous dispersions or as compositions consisting of dissolved lipids. It is an object of the present invention to provide a new improved system to administer liposomal formulations. The invention is based on the fact that certain lipid-based solid materials hydrate to form or reconstitute liposomes in an aqueous milieu. The lipid-based solid materials are administered to the body in aerosol form by a suitable device and the hydration to liposomes occurs in vivo, either at the site of action or elsewhere.

Although the aerosolized lipid-based solid material can be administered to various parts of the body applications where it is inhaled as a finely-divided powder and hydrated in the respiratory tract are particularly suitable. It is therefore a further object of the present invention to

provide a pharmaceutical package suitable for inhalation therapy.

5 Background art

Liposomes

10 Liposomes are widely described in the literature and their general structure is well known, they are structures composed of concentric rings of lipid bilayers. Liposomes have been used as carriers for different kinds of pharmacologically active substances in order to improve their therapeutic efficacy.

15 Liposomes can be used as carriers both for hydrophilic and lipophilic substances. Hydrophilic substances are encapsulated in the aqueous space between the lipid bilayers while lipophilic substances are incorporated into the lipid
20 bilayers.

Liposomes can be made from a range of lipids, both neutral and charged, including phosphatidylcholines, and can be manufactured in a number of different ways resulting in
25 liposomes with various properties. Liposomes can therefore to some extent be tailored to suit a specific application. Examples of parameters which can be controlled are liposome size (20 nm - 10 μ m), type [SUV (small unilamellar vesicles), LUV (large unilamellar vesicles), MLV (multilamellar
30 vesicles) etc], phase-transition temperature, T_c (and hence the rate of release of encapsulated substance) and liposome charge.

One of the major problems in the development of a pharmaceutical liposomal formulation is the long-time stability.
35 Aqueous liposome dispersions have a limited physical stability since the liposomes can aggregate resulting in a

change in the size distribution. Furthermore, if the encapsulated drug is hydrophilic it may be lost into the external aqueous phase. In addition, there is a potential risk for chemical degradation of the lipid components and the pharmacologically active substance in an aqueous milieu.

One way to circumvent the physical stability problem is to store the lipid dissolved in an organic solvent and form liposomes immediately before use. However, also with this approach chemical degradation can be a problem.

The problem concerning stability can to large extent be solved if a dry solid composition is developed. The term "dry" implies a virtually water-free formulation but does not imply the absence of a liquid in which the solid composition is virtually insoluble. A dry solid composition is stable during long time at room temperature and under moisture protection in a closed container.

Two different approaches to provide dry solid compositions have been suggested. The first approach is by liposome precursors, proliposomes. Proliposomes are formulations from which liposomes readily can be prepared, usually by dispersing the proliposome material in an aqueous solution and, if necessary, heating the dispersion to a temperature above the phase-transition temperature of the lipid material (UK Patent Specification 1 575 343, UK Patent Application GB 2 135 268 A).

The second approach to obtain a dry solid composition is to dehydrate a liposome dispersion in the presence of a filler material intended to impede agglomeration of the dehydrated product (UK Patent Application GB 2 002 319 A). The dehydration can for example be performed by lyophilization or by spray-drying. The liposomes are reconstituted by rehydration of the dry product.

The dry solid products of the both approaches discussed above can be used in the present invention. Instead of hydrating the dry solid material before administration as in previous methods, it is in the present invention administered to the body in aerosol form by a suitable device. In the body the dry lipid-based solid material is hydrated to liposomes.

10 Inhalation therapy

The administration of pharmacologically active substances by inhalation has been known and employed for many years. For many conditions, especially those which involve allergic and inflammatory diseases in the respiratory tract, inhalation of drugs can be exceedingly useful.

Various inhalation devices such as powder-inhalators (Spinhaler[®], Rotahaler[®], Turbuhaler[®] etc) and pressurized dose-aerosols exist. A powder-inhalator provides a selected quantity of a dry powder in a form suitable for inhalation. No powder-inhalators containing a lipid-based solid material exist.

The pressurized dose-aerosol is a pressure-tight container having a valve-controlled opening and containing a self-propelling composition capable of providing drug in aerosol form. The self-propelling composition comprises a propellant in which the pharmacologically active substance is dissolved or dispersed. Optionally, adjuvants such as ethanol, nonionic surfactants, taste maskers, etc are added to improve the formulation. On operating the metering valve of the aerosol container, the active material is dispensed in a stream of propellant. Pressurized dose-aerosols containing lipid materials exist on the market. However, these materials are present as suspending agents for the drug particles in the propellant and as valve lubricants.

UK Patent Application GB 2 145 107 A provides a method and a pack for in situ formation of liposomes in which at least two separate components are brought together under pressure, the first component comprising water and the second component comprising a dissolved lipid material. The components are passed as a mixture through a nozzle or other arrangement to produce an aerosol spray containing liposomes.

European Patent Application 158 441 provides aerosol compositions comprising in a volatile liquid propellant

a) at least one membrane lipid

b) at least one water-miscible liquid which is a solvent for the lipid, and

c) optionally water and/or a biologically active substance.

When the composition is sprayed, the propellant volatilises, leaving an aerosol of the remaining components as a proliposome composition in the form of droplets. In the presence of water, these droplets spontaneously form liposomes.

PCT application WO 86/01714 describes a process for the preparation of liposomes which comprises spraying micro-fine droplets of substantially pure phospholipid in a volatile liquid carrier to impinge either upon or below an aqueous surface thereby forming liposomes. The volatile liquid carrier is preferably a solvent for the phospholipid and the drug molecules must be dissolved in the formulation.

The aerosol compositions described above differ from the present invention in that the lipid material and/or the biologically active material are not in a particulate solid state, but dissolved in a solvent. As mentioned above

chemical stability can be a large problem when the lipid material and or the biologically active substances are in a dissolved state.

5

Detailed description of the present invention

10 The present invention provides a new system to administer liposomal formulations to mammals, including man. The system comprises a dry lipid-based solid material and a device for aerosolizing said material. The said material can either be manufactured by dehydration of a liposome dispersion in the presence of a filler material or be a proliposome material. The said materials spontaneously
15 hydrate to form or reconstitute liposomes at the target organ or elsewhere in the body. The device is preferable a breath-actuated powder-inhalator or a pressurized dose-aerosol. The present method is distinguished from previous methods to administer liposomal formulations in that the
20 lipid-based composition is, not dissolved in a solvent or dispersed in water, but in a particulate solid state. The problems concerning chemical stability are therefore eliminated.

25 The dry lipid-based solid materials used in the present invention contain lipid material and optionally a pharmacologically active substance. They can also contain at least one adjuvant which imparts advantageous properties.

30 The lipid material can be any of those conventionally used in liposomal formulations. Usually the main liposome-forming component is a phospholipid, including synthetic lecithins and natural lecithins. In addition to the main liposome-forming component other lipids may be used to optimize
35 the properties of the formulation. Examples of such additives are sterols such as cholesterol or derivatives thereof or components with a positive or negative charge.

Cholesterol or derivatives thereof may be incorporated, preferably in a proportion of 0.1 to 50 % w/w of the total lipids, to modify the membrane structure rendering it more fluid or more rigid and thereby influence the release properties of the entrapped pharmacologically active material. Cholesterol also has a positive effect on the stability of the liposomes during lyophilization.

Components with a negative or positive charge will provide an electrostatic stabilization of the liposomes and may also improve the uptake of the liposomes in the target cells. Examples of negatively charged lipophilic substances are phosphatic acid, dicetyl phosphoric acid, phosphatidyl serine, phosphatidyl inositol and phosphatidyl glycerol. Examples of positively charged lipophilic substances are stearylamine, stearylamine acetate and cetylpyridinium chloride.

Both hydrophilic and lipophilic pharmacologically active substances can be encapsulated into the liposomes. Alternatively, liposomes can be made without any encapsulated substance.

Suitable adjuvants are filler substances such as carbohydrates, for example lactose, sucrose or trehalose. These materials facilitate the dispersion of a proliposome material and impede agglomeration of a dehydrated product.

The proliposome formulation used in the present invention can be any which in an aqueous milieu forms liposomes in the temperature range of current interest. Some care must be taken to ensure that liposomes and not other structures are formed when a proliposome material is used.

A material obtained from a dehydrated liposome dispersion gives larger opportunities to tailor the formulation. The liposome dispersion from which the dry solid material is

made can be prepared according to any of the numerous methods known in the art. The dehydration can be performed with any method which does not destroy the liposomal structure. Preferably, the dehydration will be carried out by lyophilization or spray-drying in the presence of a filler material.

The system described in the present invention can be used to administer liposomes to various parts of the body. The following routes of administration should be mentioned; oral, rectal, vaginal, in open wounds, and by inhalation. For each application the system must be optimized both with respect to the lipid-based solid composition (components, method of manufacture etc) and the device (breath-actuator powder-inhalator, pressurized aerosol etc).

Inhalation therapy is an attractive application of the present invention. In the respiratory tract there is a large area with high humidity where the lipid-based solid material can be hydrated. Various powder-dispensing devices such as powder-inhalators and pressurized dose-aerosols which can deliver a powder of the material to the respiratory tract exist.

Pharmacologically active substances which are particularly useful for inhalation are β_2 -receptor active substances, xanthines, glucocorticoids, other antiallergic or anti-inflammatory substances or derivatives of the substances mentioned.

Suitable β_2 -receptor active substances are terbutaline, salbutamol, mabuterol, fenoterol, formoterol, orciprenaline, isoprenaline, isoetharine, clenbuterol, hexoprenaline, procaterol, 1-(4-hydroxyphenyl)-2-[1,1-dimethyl-3-(2-methoxyphenyl) propylamino]-ethanol, 1-(3,5-dihydroxyphenyl)-2-[1,1-dimethyl-3-(2-methoxyphenyl) propylamino]-ethanol, 1-3,4-dihydroxyphenyl)-2-[1,1-dimethyl-3-(2-methoxyphenyl) propylamino]-ethanol, (4-hydroxy- α' -[[[6

5 -(4-phenylbutoxy)-hexyl]-amino]-methyl]-1,3 benzyldimethanol, pharmacologically acceptable salts or derivatives thereof and compounds of similar pharmacological properties. The β_2 -receptor active substance which is particularly preferred is terbutaline sulphate.

10 Among the xanthines theophylline and enprofylline and pharmacologically acceptable salts and derivatives thereof and compounds of similar pharmacological properties are the most suitable.

15 Suitable glucocorticoids are compounds like budesonide, beclomethasone, dexamethasone, flumethasone, flunisolide, triamcinolone acetonide, 17- and/or 21-esters of these steroids, pharmacologically acceptable salts thereof and compounds of similar pharmacological properties.

20 Other compounds which can be used in accordance with the present invention are cromoglycate, lidocaine, indometacin, diclofenac, ibuprofen, piroxicam, sulindac, derivatives thereof and compounds of similar pharmacological properties.

25 Breath-actuated powder-inhalers are suitable devices to administer the lipid-based solid material to the respiratory tract. As said material may be sensitive to moisture it may be necessary to ensure moisture protection. This is also the case for certain other inhalation materials on the market, for example sodium cromoglycate, and can therefore easily be ensured also for said solid-based lipid material.

30 The pressurized dose-aerosol is for several reasons, which will be discussed below, a particular suitable device. Considerations which must be taken into account when a pressurized dose-aerosol is developed are therefore discussed below.

35

The pressurized dose-aerosol can be manufactured according to known technique i.e. a powder of a defined particle-size is suspended in a suitable propellant mixture. The dispersion is filled on containers which are sealed with a metering valve. The water content should be kept as low as possible. The components making up the lipid-based solid composition must be virtually insoluble in the propellant. Further they must of course be chemically stable during storage in the aerosol container. (Since the components are insoluble in the propellant mixture this is generally no problem.) It is often necessary to exclude propellant 11 (CCl_3F) from the formulation since it has the highest solvency power among the propellants which normally are used in pressurized dose-aerosols for medicinal use. By mixing propellant 12 (CCl_2F_2) and propellant 114 ($\text{CClF}_2\text{CClF}_2$) in different proportions pressurized dose-aerosols with the desired pressure can be obtained. If necessary it is possible to minimize the solubility of the solid components by using propellant 115 (CClF_2CF_3) or propellant C-318 (C_4F_8). These are among the poorest solvents known. Preferably the solid material is suspended in a concentration between 0.001 and 20 % by weight, in the liquified propellant.

The pressurized dose-aerosol can also contain at least one adjuvant which imparts advantageous properties. Such adjuvants may be surfactants, taste-maskers or modifiers of the solubility of the lipid-based solid material in the propellant. Preferred surfactants are those which are soluble in the propellant and constitutes between 0.001 % and 20 % by weight of the total composition.

The solubilities of a range of lipids and pharmacologically active substances in different propellants have been measured. The substance was dispersed in the propellant and the sample was stored in a sealed container under pressure. After equilibrium the sample was filtered and the concentration was determined. Some of the results are presented in Table 1.

Table 1 Solubilities in propellants/ $\mu\text{g} \times \text{g}^{-1}$

	<u>Propellant</u>		
	12	114	115
5			
	budesonide-21-palmitate	170	
10	flunisolide-21-palmitate	60	12
	flumethasone-21-palmitate	5.9	1.0 < 0.005
	flumethasone-21-stearate	2.4	1.5
15	DPFC (dipalmitoyl phosphatidylcholine)		< 2
	DMPC (dimyristoyl phosphatidylcholine)		< 2
20	Epikuron [®] 200 H (> 95 % phosphatidylcholine, Lucas Meyer, Hamburg)		< 2
25	DPPA (dipalmitoyl phosphatic acid)		< 10
	Stearylamine		< 10
30	Catalase		< 10

It can be seen from the table that the solubilities of many important substances are very low in the propellants making a suspension aerosol feasible.

The pressurized dose-aerosol described above shows advantages compared to other ways of storing and delivering liposomal formulations. It comprises a package where the material is protected during storage from air, light, moisture etc, which may affect the material. It is easy to administer a dose of the formulation without affecting the rest of the material. The lipid material is in a solid state and therefore there is minimal risk for chemical degradation and for changes in the physical structure.

There is no need for expensive aerosol-delivering devices as ordinary aerosol containers and valves can be used (in contrast to technical approaches where special devices are needed to mix the lipid material with an aqueous solution). Finally, the liposomes can be manufactured to have specific properties (liposome size, drug-loading etc) which may be difficult to obtain when the liposomes are generated in situ.

Working examples

The present invention is exemplified but in no way limited by the following examples. A variety of other materials and other methods could be used to obtain the desired lipid-based solid composition. Further, other routes and devices could be used to administer the lipid-based solid material. In all examples care was taken to avoid that the dry solid formulation came into contact with moisture.

Example 1

1 g DPPC was dissolved in 50 ml t-butanol under gentle heating. The solution was frozen and lyophilized. The resulting powder was dispersed in 135 g of a sterile aqueous solution of lactose (6.67 weight %). Liposomes were formed by heating (maximum temperature 75 °C) the sample for 45 minutes during stirring. The liposome dispersion was flash-

frozen by dripping it into liquid nitrogen and was then lyophilized. The dry powder was micronized to a particle-size suitable for inhalation therapy (MMD < 3 μ m according to image-analysis). A number of gelatine capsules were each
5 filled with 20 mg of the lyophilized and micronized lipid composition. Other gelatine capsules were filled with 20 mg of micronized lactose. The capsules were used to determine the tolerance of inhaling the lipid-based solid composition in man using a randomized, single blind cross-over study.
10 The powders were administered by inhalation using Spin-matic[®] inhalator to 10 healthy volunteers. Each volunteer received 3 single doses of the two formulations. There was a wash-out period of at least 2 days between the treatments. No adverse drug experiences (ADE) were found in the
15 study.

Example 2

20 10 g Epikuron[®] 200 H (Lucas Meyer, Hamburg) was dissolved in 100 g t-butanol under gentle heating. The solution was frozen and lyophilized. 3 g of the resulting powder was dispersed in 270 g of an aqueous solution of lactose (6.67 weight %). Liposomes were formed by heating (maximum temperature 75 °C) the sample for approximately 30 minutes
25 during stirring. The liposome dispersion was flash-frozen by dripping it into liquid nitrogen and was then lyophilized. The dry powder was micronized to a particle-size suitable for inhalation therapy (MMD < 3 μ m according to image-analysis). 2 g of the lyophilized and micronized
30 powder was agglomerated to spheres with a diameter of less than 1 mm. This gives a powder with improved flow-properties. The agglomerated powder was filled into powder-inhalers (Turbuhaler[®], United States Patent 4,524,769). The
35 powder-inhaler is designed to dispense the agglomerated substance accurately. Inspiration through the Turbuhaler[®]

hence leads to inhalation of a certain amount of the powder.

5 Example 3

In a 2 l flask 2 g Epikuron[®] 200 H was dissolved in 20 ml chloroform. The chloroform was evaporated to leave a lipid film on the inner surface of the flask. 110 g of an aqueous solution of lactose (9.1 weight %) was added. Liposomes were formed by shaking the flask at elevated temperature. The liposome-dispersion was spray-dried with a Buchi 190 Mini Spray-Dryer using an inlet temperature of 155 °C. The final traces of water were eliminated by over-night storage under reduced pressure (0.1 torr). The particle size of the spray-dried powder was suitable for inhalation therapy (MMD < 3 µm according to image-analysis). 100 mg of the powder was dispersed in 10 g of a chilled 50:50 w/w mixture of propellant 12 and propellant 114. The mixture was sealed in a glass container fitted with a 50 µl metering valve. The resulting pressurized dose-aerosol was used to produce an aerosol which formed liposomes in an aqueous milieu.

25 Example 4

1.43 g of a lyophilized Epikuron[®] 200 H powder (lyophilized from t-butanol as described above) was dispersed in 500 g of an aqueous solution of lactose containing 8.57 g lactose. Liposomes were formed by heating (maximum temperature 70 °C) the sample for 45 minutes during stirring. The liposome dispersion was spray-dried with a Buchi 190 Mini Spray-Dryer using an inlet temperature of 155 °C. The final traces of water were eliminated by over-night storage under reduced pressure (0.1 torr). The particle size of the spray-dried powder was suitable for inhalation therapy (MMD < 3 µm according to image-analysis). 100 mg of the

powder was dispersed in 10 g of a chilled 50:50 w/w mixture of propellant 12 and propellant 114. The mixture was sealed in an glass container fitted with a 50 μ l metering valve. The resulting pressurized dose-aerosol was used to produce an aerosol which formed liposomes in an aqueous milieu.

Example 5

The procedure of example 4 was repeated except that 3.33 g of lyophilized Epikuron[®] 200 H powder was dispersed in 500 g of an aqueous solution of lactose containing 6.67 g lactose. The resulting pressurized dose-aerosol was used to produce an aerosol which formed liposomes in an aqueous milieu.

Example 6

The procedure of example 5 was repeated except that a lyophilized mixture of DPPC and flumethasone-21-palmitate (19:1 w/w) was used instead of Epikuron[®] 200 H. The resulting pressurized dose-aerosol was used to produce an aerosol which formed liposomes in an aqueous milieu.

Example 7

3.04 g DPPC and 0.16 g flumethasone-21-stearate were dissolved in 65 g t-butanol under gentle heating. The solution was frozen and lyophilized. The resulting powder was dispersed in 245 g of an aqueous solution of lactose (6.67 weight %). Liposomes were formed by heating (maximum temperature 70 °C) the sample for at least 30 minutes during stirring. The liposome dispersion was flash-frozen by dripping it into liquid nitrogen and was then lyophilized. The dry powder was micronized to a particle-size suitable

for inhalation therapy (MMD < 3 μ m according to image-analysis). 5.0 g of the lyophilized and micronized powder was dispersed in 340 g of a chilled 50:50 w/w mixture of propellant 12 and propellant 114. Containers were filled with approximately 10 g each of the suspension and sealed. Both Al-containers and glass containers were used. 50 μ l valves with steam of stainless steel, 50 μ l valves with steam of plastic and non-metering valves were used to seal the containers. The resulting pressurized dose-aerosols were used to produce an aerosol which formed liposomes in an aqueous milieu.

Example 8

17.1 g DPPC and 0.9 g flumethasone-21-palmitate were dissolved in 360 g t-butanol under gentle heating. The solution was frozen and lyophilized. 9.5 g of the dry lyophilized powder was dispersed in 812 g of an aqueous solution of lactose (6.67 weight %). Liposomes were formed by heating (maximum temperature 70 °C) the sample for approximately 1 hour during stirring. The liposome dispersion was flash-frozen by dripping it into liquid nitrogen and was then lyophilized. The dry powder was micronized to a particle-size suitable for inhalation therapy (MMD < 3 μ m according to image-analysis). 16.3 g of the lyophilized and micronized powder was dispersed in 1100 g of a chilled 50:50 w/w mixture of propellant 12 and propellant 114. Containers were filled with approximately 8.7 g each of the suspension and sealed. Both Al-containers and glass containers were used. 50 μ l valves with steam of stainless steel, 50 μ l valves with steam of plastic and non-metering valves were used to seal the containers. The resulting pressurized dose-aerosols were used to produce an aerosol which formed liposomes in an aqueous milieu.

Example 9

16.0 g of the lyophilized and micronized powder manufactured in example 8 was dispersed in 1100 g of a chilled
5 65:35 w/w mixture of propellant 114 and propellant 115. Containers were filled with approximately 8.7 g each of the suspension and sealed. Both Al-containers and glass containers were used. 50 μ l valves with steam of stainless
10 steel, 50 μ l valves with steam of plastic and non-metering valves were used to seal the containers. The resulting pressurized dose-aerosols were used to produce an aerosol which formed liposomes in an aqueous milieu.

15 Example 10

The procedure of Example 8 was repeated except that 7.5 g of the dry powder resulting from the lyophilization of the
20 t-butanol solution in that example was dispersed in 314 g of an aqueous solution of lactose (4.78 weight %). Furthermore, 7 g of the lyophilized and micronized powder was dispersed in the propellant mixture. The resulting pressurized dose-aerosols were used to produce an aerosol which formed
25 liposomes in an aqueous milieu.

Example 11

6.0 g of the lyophilized and micronized powder manufactured
30 in example 10 was dispersed in 1100 g of a chilled 65:35 w/w mixture of propellant 114 and propellant 115. Containers were filled with approximately 8.7 g each of the suspension and sealed. Both Al-containers and glass containers were used. 50 μ l valves with steam of stainless steel,
35 50 μ l valves with steam of plastic and non-metering valves were used to seal the containers. The resulting pressurized

dose-aerosols were used to produce an aerosol which formed liposomes in an aqueous milieu.

5 Example 12

10 parts of DPPC and 1 part of budesonide-21-palmitate were dissolved in 500 parts of t-butanol under gentle heating. The solution was frozen and lyophilized. 1.38 g of the re-
10 sulting powder was dispersed in 168 g of an aqueous solution of lactose (10.0 weight-%). Liposomes were formed by heating (maximum temperature 60 °C) the sample for approximately 30 minutes during stirring. The liposome dispersion was flash-frozen by dripping it into liquid nitrogen and
15 was then lyophilized during three days. The dry powder was micronized to a particle-size suitable for inhalation therapy (MMD < 3 µm according to image-analysis). 4.35 g of the lyophilized and micronized powder was dispersed in
20 500 g of a chilled 50:50 w/w mixture of propellant 12 and propellant 114. Containers were filled with approximately 9 g each of the suspension and sealed. Both Al-containers and glass containers were used. 50 µl valves with stem of stainless steel, 50 µl valves with stem of plastic and non-metering valves were used to seal the containers. The
25 resulting pressurized dose-aerosols were used to produce an aerosol which formed liposomes in an aqueous milieu.

Example 13

30

5 g Epikuron[®] 200 H was dissolved in 135 g t-butanol under gentle heating. The solution was frozen and lyophilized. 4 g of the dry lyophilized powder was dispersed in 200 g distilled water. Liposomes were formed by heating (maximum
35 temperature 70 °C) the sample for 1 hour during stirring. 2 g terbutaline sulphate was dissolved in 100 g distilled water. The both preparations were mixed, frozen and lyo-

philized. 5 g of the dried product was dispersed in 27 ml distilled water. Liposomes were formed by heating (maximum temperature 70 °C) the samples for 30 minutes under stirring. The dispersion was diluted with 350 g of an aqueous solution of lactose (6.67 weight %). The liposome dispersion was flash-frozen by dripping it into liquid nitrogen and was then lyophilized. The dry powder was micronized to a particle-size suitable for inhalation therapy (MMD < 3 μ m according to image-analysis). The encapsulation of terbutaline sulphate into the liposomes was measured spectrophotometrically at 280 nm. It was found to be 33 % both before and after micronization. 4.8 g of the lyophilized and micronized powder was dispersed in 556 g of a chilled 50:50 w/w mixture of propellant 12 and propellant 114. Al-containers were filled with approximately 14 g of the suspension and sealed with metering valves. The resulting pressurized dose-aerosols were used to produce an aerosol which formed liposomes in an aqueous milieu.

20

Example 14

100 mg DMPC dissolved in 1 ml chloroform was added to a flask. The chloroform was evaporated to leave a thin lipid film on the inner surface of the flask. 4 ml distilled water was added. Liposomes were formed by shaking the flask at 35 °C. 100 mg of a protein (catalase) dissolved in 1 ml distilled water was added. The sample was frozen and lyophilized. The resulting powder was dispersed in 1 ml distilled water at 35 °C. When liposomes had formed the sample was diluted with 5 ml of an aqueous solution of lactose containing 500 mg lactose. The liposome dispersion was flash-frozen by dripping it into liquid nitrogen and was then lyophilized. The encapsulation of catalase into the liposomes was determined spectrophotometrically at 280 nm to 25 %. 100 mg of the powder was dispersed in 10 g of a chilled 50:50 w/w mixture of propellant 12 and propellant

114. The mixture was sealed in a glass container fitted with a 50 μ l metering valve. The resulting pressurized dose-aerosol was used to produce an aerosol which formed liposomes in an aqueous milieu.

5

Example 15

10 The procedure of example 14 was repeated except that DPPC was used instead of DMPC and a xantine (caffeine) was used instead of catalase. Furthermore, the temperature was 60 °C during formation of the liposomes. The resulting pressurized dose-aerosol was used to produce an aerosol which formed liposomes in an aqueous milieu.

15

Example 16

20 40 mg DMPC was dissolved in 5 g t-butanol under gentle heating. The solution was frozen and lyophilized. The resulting powder was dispersed in 15 g of a chilled 50:50 w/w mixture of propellant 12 and propellant 114. The mixture was sealed in a glass container fitted with a 50 μ l metering valve. The resulting pressurized dose-aerosol was used to produce an aerosol which formed liposomes in an aqueous milieu.

25

Example 17

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40 mg DMPC and 2 mg flumethasone-21-palmitate were dissolved in 5 g t-butanol under gentle heating. The solution was frozen and lyophilized. The resulting powder was dispersed in 15 g of a chilled 50:50 w/w mixture of propellant 12 and propellant 114. The mixture was sealed in a glass container fitted with a 50 μ l metering valve. The resulting

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pressurized dose-aerosol was used to produce an aerosol which formed liposomes in an aqueous milieu.

5 Example 18

7.22 g DPPC and 0.38 g flumethasone-21-palmitate were dissolved in 76 g t-butanol under gentle heating. The solution was frozen and lyophilized. The resulting powder was dispersed in 432 g of an aqueous solution of lactose (3.33 weight %). Liposomes were formed by heating (maximum temperature 65 °C) the sample for at least 30 minutes during stirring. The liposome dispersion was spray-dried with a Buchi 190 Mini Spray-Dryer using an inlet temperature of 155 °C. The particle size of the spray-dried powder was suitable for inhalation therapy (MMD < 3 µm according to image-analysis). 2.8 g of the lyophilized and micronized powder was dispersed in 434 g of a chilled 65:35 w/w mixture of propellant 114 and propellant 115. Al-containers were filled with approximately 16.7 g each of the suspension and sealed with 50 µl valves.

The resulting pressurized dose-aerosols were used to produce an aerosol which groups of Sprague Dawley rats were exposed to nose-only in a Battelle inhalation chamber. After the first exposure, the animals were given Sephadex beads by intratracheal instillation. The animals were then exposed to the aerosol daily for three consecutive days. On the fifth day the animals were sacrificed and the lung weights were examined.

Animals given Sephadex beads and treated with placebo pressurized dose-aerosols (containing the same components as described above except for the spray-dried powder) developed pulmonary edema measured as increased lung weight. Groups of animals treated with three different doses from the pressurized dose-aerosols showed a significant dose-

response relationship. The high dose level inhibited the development of lung edema and the animals showed the same lung weight as the normal rats in the control group.

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CLAIMS

- 1) A system for administration of a lipid-based material to mammals, including man characterized in that it comprises a dry lipid-based solid material in a particulate form, which forms or reconstitutes liposomes in the presence of water, and a device suitable to administer said solid material as an aerosol.
- 2) A system as claimed in claim 1 wherein the main lipid component of the solid material is one or more phospholipids, eg phosphatidylcholine optionally together with one or more other lipid components.
- 3) A system as claimed in any one of claims 1 to 2 wherein the solid material contains a sterol and/or a substance which donates a positive or a negative charge to the liposomes.
- 4) A system as claimed in any one of claims 1 to 3 wherein the solid material contains a pharmacologically active substance or derivatives thereof.
- 5) A system as claimed in claim 4 wherein the pharmacologically active substance or derivative thereof is entrapped within the liposomes which are formed or reconstituted from the dry lipid-based solid material or partitioned between the liposomes, which are formed or reconstituted from the dry lipid-based solid material, and an external phase.
- 6) A system as claimed in any one of claims 4 to 5, wherein the pharmacologically active substance is a β_2 -receptor active substance, preferably selected from the following substances: terbutaline, salbutamol, mabuterol, fenoterol, formoterol, orciprenaline, isoprenaline, isoetharine, clenbuterol, hexoprenaline, proca-

terol, 1-(4-hydroxyphenyl)-2-[1,1-dimethyl-3-(2-methoxyphenyl) propylamino]-ethanol, 1-(3,5-dihydroxyphenyl)-2-[1,1-dimethyl-3-(2-methoxyphenyl) propylamino]-ethanol, 1-3,4-dihydroxyphenyl)-2-[1,1-dimethyl-3-(2-methoxyphenyl) propylamino]-ethanol, (4-hydroxy-
5 - α' -[[[6-(4-phenylbutoxy)-hexyl]-amino]-methyl]-1,3 benzyldimethanol, or a pharmacologically acceptable salt or derivative of any one thereof and mixtures thereof.

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7) A system as claimed in claim 6 wherein the β_2 -receptor active substance is terbutaline sulphate.

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8) A system as claimed in any one of claims 4 to 5 wherein the pharmacologically active substance is a glucocorticosteroid, preferably selected from the following substances: budesonide, beclomethasone, dexamethasone, flumethasone, triamcinolone acetonide, flunisolide, 17-
20 and/or 21-esters of these steroids or a pharmacologically acceptable salt of any one thereof and mixtures thereof.

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9) A system as claimed in claim 8 wherein the glucocorticosteroid is a 21-fatty acid ester of budesonide or flumethasone.

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10) A system as claimed in any one of claims 4 to 5, wherein the pharmacologically active substance is a xanthine such as theophylline or enprofylline, or cromoglycate, lidocaine, indometacin, diclofenac, ibuprofen, piroxicam, sulindac, or a pharmacologically acceptable salt or derivative of any one thereof and mixtures thereof.

- 11) A system as claimed in any one of claims 1 to 10 where-
in the solid material contains a filler material, pre-
ferably a carbohydrate, eg lactose, trehalose or suc-
rose.
- 5 12) A system as claimed in any one of claims 1 to 11 where-
in the solid material is manufactured by dehydration of
a liposome dispersion preferably by lyophilization or
spray-drying.
- 10 13) A system as claimed in any one of claims 1 to 12 where-
in the solid material is administered by any of the
following routes; oral, rectal, vaginal, in open
wounds, or by inhalation.
- 15 14) A system as claimed in any one of claims 1 to 13 where-
in the solid material has a particle size such as at
least 95 % by weight is less than 10 microns in
diameter.
- 20 15) A system as claimed in any one of claims 1 to 14 where-
in the solid material is administered by means of a
powder-inhalator.
- 25 16) A system as claimed in any one of claims 1 to 14 where-
in the solid material is administered by means of a
self-propelling powder-dispensing composition.

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- 17) A system as claimed in claim 16 wherein the self-propelling powder dispensing aerosol composition comprises a liquefied propellant in which said solid material is substantially insoluble, preferably a halogenated hydrocarbon eg
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- propellant 12 (CCl_2F_2)
propellant 114 ($\text{CClF}_2\text{CClF}_2$)
propellant 115 (CClF_2CF_3)
10 or propellant C-318 (C_4F_8)
- or a mixture of halogenated hydrocarbons.
- 18) A package comprising a pressure-tight container having a valve-controlled opening and containing a solid material and a self-propelling powder-dispensing composition as claimed in any one of claim 16 to 17.
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- 19) A pharmaceutical package as claimed in claim 18 capable of providing a measured dose of medicament in aerosol form suitable for inhalation therapy.
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- 20) Use of a system according to any of claims 1 to 17 or a package according to any of claims 18 to 19 for administration of lipid-based material to mammals, including man.
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INTERNATIONAL SEARCH REPORT

International Application No PCT/SE87/00401

I. CLASSIFICATION OF SUBJECT MATTER (if several classification symbols apply, indicate all) *		
According to International Patent Classification (IPC) or to both National Classification and IPC 4		
A 61 K 9/12, 9/72, 31/685, 47/00		
II. FIELDS SEARCHED		
Minimum Documentation Searched 7		
Classification System	Classification Symbols	
IPC 4	A 61 K 9/00, /12, /50, /72, 47/00, 31/685, 37/22	
US C1	264: 4.1-4.7; 424: 19, 38, 46	
Documentation Searched other than Minimum Documentation to the Extent that such Documents are Included in the Fields Searched *		
SE, NO, DK, FI classes as above		
III. DOCUMENTS CONSIDERED TO BE RELEVANT *		
Category *	Citation of Document, 11 with indication, where appropriate, of the relevant passages 12	Relevant to Claim No. 13
X,Y	EP, A, 158 441 (PHARES PHARMACEUTICAL RESEARCH N V) 16 October 1985 see claims 1-12, 14, page 7, lines 31-37, page 8, lines 5-21, examples & JP, 61044808	1-6,8,10, 11, 13-16
Y	SE, A, 8404118-5 (STERWIN AG) 18 February 1985 see claim 13 examples 5-7 & GB, A, 2145107	1-4, 13 15-19
Y	GB, A, 1 575 343 (IMPERAIL CHEMICAL INDUSTRIES LTD) 17 September 1980 see claims, page 2, lines 72-91, examples & NL, 7805005 BE, 866697 FR, 2390159 DE, 2818655 JP, 53142514 US, 4311712 AU, 514644 .../...	1-4, 12
<p>* Special categories of cited documents: 10</p> <p>"A" document defining the general state of the art which is not considered to be of particular relevance</p> <p>"E" earlier document but published on or after the international filing date</p> <p>"L" document which may throw doubts on priority claim(s) or which is cited to establish the publication date of another citation or other special reason (as specified)</p> <p>"O" document referring to an oral disclosure, use, exhibition or other means</p> <p>"P" document published prior to the international filing date but later than the priority date claimed</p> <p>"T" later document published after the international filing date or priority date and not in conflict with the application but cited to understand the principle or theory underlying the invention</p> <p>"X" document of particular relevance; the claimed invention cannot be considered novel or cannot be considered to involve an inventive step</p> <p>"Y" document of particular relevance; the claimed invention cannot be considered to involve an inventive step when the document is combined with one or more other such documents, such combination being obvious to a person skilled in the art.</p> <p>"A" document member of the same patent family</p>		
IV. CERTIFICATION		
Date of the Actual Completion of the International Search	Date of Mailing of this International Search Report	
1987-11-10	1987 -11- 16	
International Searching Authority	Signature of Authorized Officer	
Swedish Patent Office	Agneta Tannerfeldt	

FURTHER INFORMATION CONTINUED FROM THE SECOND SHEET

V. ☒ OBSERVATIONS WHERE CERTAIN CLAIMS WERE FOUND UNSEARCHABLE ¹

This International search report has not been established in respect of certain claims under Article 17(2) (a) for the following reasons:

1. ☒ Claim numbers 20, because they relate to subject matter not required to be searched by this Authority, namely:

Methods for treatment of the human or animal body by therapy (Rule 39.1 iv)

2. ☐ Claim numbers _____, because they relate to parts of the international application that do not comply with the prescribed requirements to such an extent that no meaningful international search can be carried out, specifically:

3. ☐ Claim numbers _____, because they are dependent claims and are not drafted in accordance with the second and third sentences of PCT Rule 6.4(a).

VI. ☐ OBSERVATIONS WHERE UNITY OF INVENTION IS LACKING ²

This International Searching Authority found multiple inventions in this international application as follows:

1. ☐ As all required additional search fees were timely paid by the applicant, this international search report covers all searchable claims of the international application.
2. ☐ As only some of the required additional search fees were timely paid by the applicant, this international search report covers only those claims of the international application for which fees were paid, specifically claims:
3. ☐ No required additional search fees were timely paid by the applicant. Consequently, this international search report is restricted to the invention first mentioned in the claims; it is covered by claim numbers:
4. ☐ As all searchable claims could be searched without effort justifying an additional fee, the International Searching Authority did not invite payment of any additional fee.

Remark on Protest

- ☐ The additional search fees were accompanied by applicant's protest.
- ☐ No protest accompanied the payment of additional search fees.

III. DOCUMENTS CONSIDERED TO BE RELEVANT (CONTINUED FROM THE SECOND SHEET)		
Category *	Citation of Document, with indication, where appropriate, of the relevant passages	Relevant to Claim No
	CA, 1114758 SE, 8201350 SE, 8201351 US, 4370349	
Y	GB, A, 1 575 344 (IMPERIAL CHEMICAL INDUSTRIES LTD) 17 September 1980 see claims, examples	1-4, 12
Y	SE, B, 440 725 (IMPERIAL CHEMICAL INDUSTRIES LTD) 19 August 1985 see claims, examples	1-4, 12
E	WO, A1, 86/06959 (LIPOSOME TECHNOLOGY INC) 4 December 1986 see claims, page 4, line 5 - page 6, line 19	1-8, 10, 12-14, 17-19